Image Acquisition - Sensors and Sources

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Outline:

- Introduction
- Benefits of Improved Sensors
- Recommendations

Existing Sensors Limit Performance!!! Example: PET

ng of Photon tectors

- Radiotracer decays by emitting a positron (β⁺).
- 511 keV photon pairs detected via time coincidence.
- Positron localized to line (defined by detector pair).
- Image reconstructed using computed tomography.
- Perfect Sensor ⇒ Time-of-Flight Localizes Positron to Point
 PET becomes PI (Positron Imaging)?

Energy per Quantum

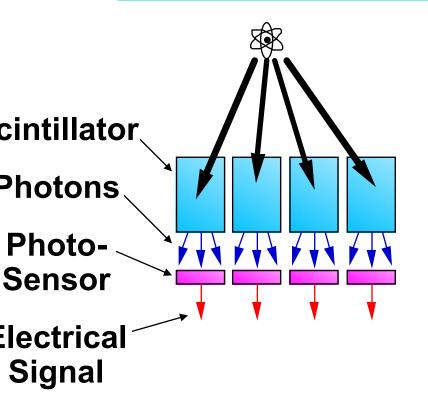
Imaging Modality	Energy / Quantum
PET	5 x 10 ⁵ eV
SPECT	1 x 10 ⁵ eV
X-Ray	5 x 10 ⁴ eV
Optical	$2 \times 10^{0} \text{ eV}$
Ultrasound	2 x 10 ⁻² eV
MRI	1 x 10 ⁻¹³ eV

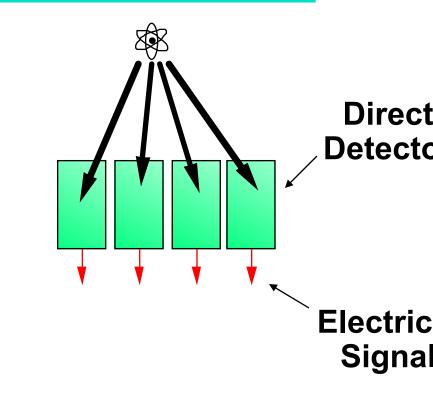
ide Range of Energies ⇒ Wide Range of Sensor

Sensors for Medical Imaging

Scintillation Detector

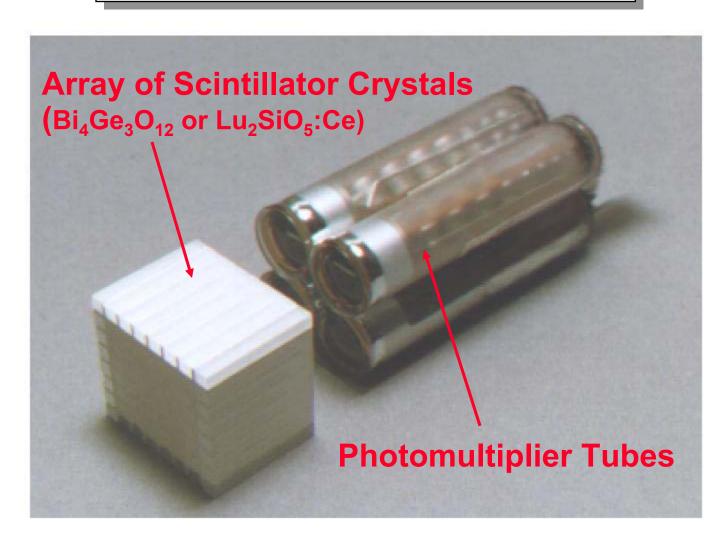
Solid State (or Direct) Detector





Sensors Are Optimized for Each Modality, But General Concepts are Identical

Typical Sensor for PET



PET Needs

Improve Timing Resolution

- Reduce Random Event Background (Up to 50% of Total Events)
- Use Time-of-Flight to Reduce Noise Variance (by 5x-10x)

Improve Energy Resolution

Scattered Events Often Outnumber True Events

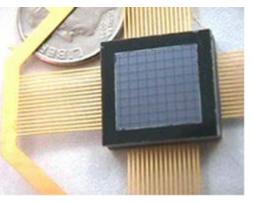
Improve Spatial Resolution

- Isotropic Resolution Throughout the Field of View
- Small Animal Imaging

SNR is Main Limitation in Clinical PET

PET: Potential Sensor Improvements





New Scintillators

- Improved Timing Resolution
- Improved Energy Resolution

Avalanche Photodiodes

- Smaller Pixels improves Spatial Resolution
- Higher Quantum Efficiency (80% vs. 25%), can improve Energy Resolution
- Better Stability

Solid State Detectors Not Useful for PET

- Too Slow (speed of sound vs. speed of light)
- High Cost per Unit Volume

New Sensors Can Improve Spatial Resolution and Significantly Reduce Background

Typical Sensor for SPECT



Photomultiplier Tubes

Scintillator Crystals (Nal:Tl)

SPECT: Needs

Improve Energy Resolution

- Reduce Scatter Background
- Over 35% of SPECT Events are Scatter

Improve Stability

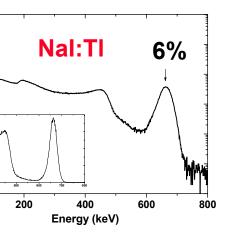
Maintain Calibration

Improve Resolution / Efficiency Tradeoff

- Set by Collimator
- Major Improvements Difficult

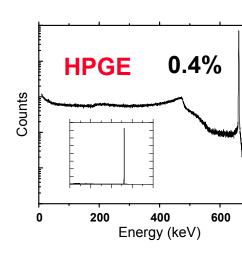
Energy Resolution is Main Limitation in SPECT

SPECT: Potential Sensor Improvements



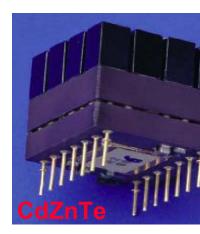
New Scintillators

Improved Energy Resolution



Solid State Detectors

- Much Improved Energy Resolution
- Improved Stability

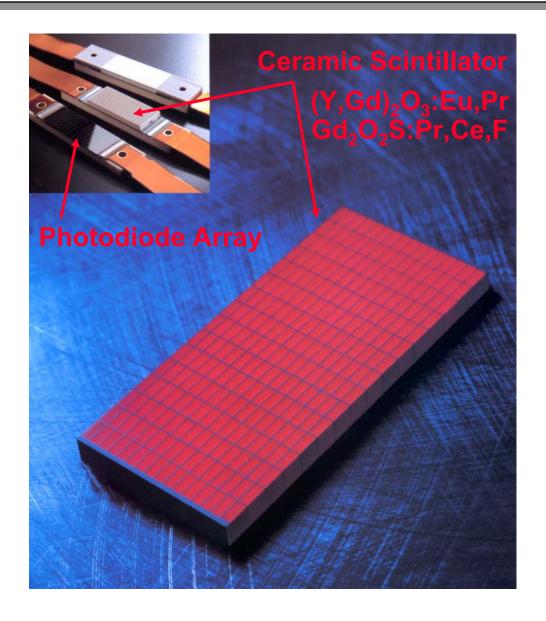


200 400 600 800 Energy (keV)

LaBr₃:Ce

est Theoretical Energy Resolution with Solid Sta

Typical Sensor for X-Ray CT



X-Ray CT: Needs

Reduced Dose

Improved Spatial Resolution

- 0.5 mm to 0.2 mm
- Difficult Without Increasing Dose or Increasing Noise

Reduced Imaging Time

Factor of 2

Scintillator & Photodetector: Little Improvement Possible

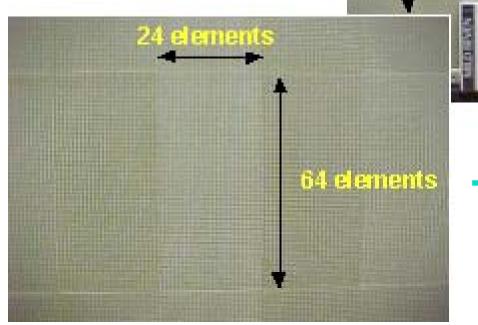
- Scintillator: High Luminous Efficiency & QE, Low Afterglow
- Photodetector: High QE, Very Stable

Main Limitation in CT is Dose

X-Ray CT: Potential Sensor Improvements

nsor: Larger 2-D Arrays

- High Channel Density (Thermal Management, Connection Density)
- Maintain Mechanical Tolerances
- Want Thinner Reflector



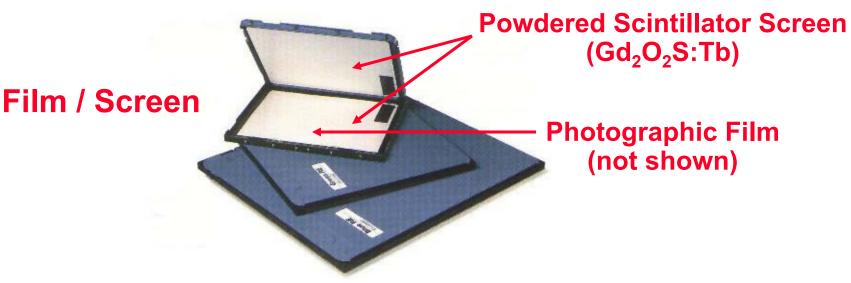
Source: Higher Power

256 elements

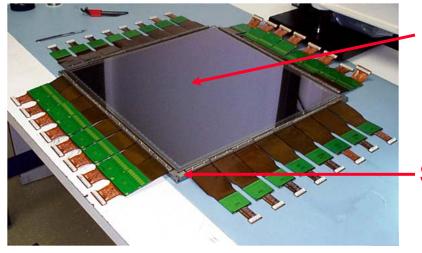
- Same Dose in Shorter Til
- Monochromatic Source?

Significant Reduction in Acquisition Time

Typical Sensor for Planar X-Ray

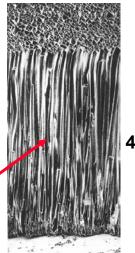


Digital

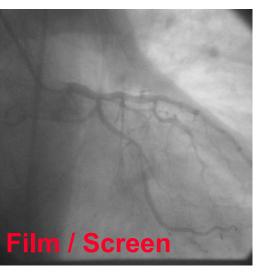


Photodiode Array

Scintillator Screen (Columnar Csl:Tl)

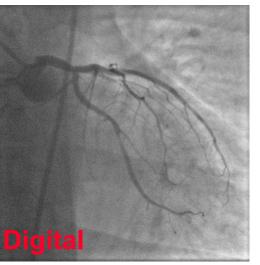


Planar X-Ray: Needs



Scintillator & Photodetector: Little Improvement Possible

- High Luminous Efficiency
- High Detective Quantum Efficiency (>70%)

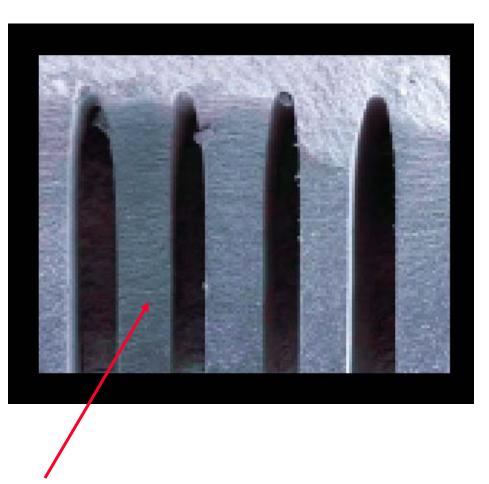


Some Improvement Possible:

- More Portable, Durable, Lighter
- Improved Falloff of DQE with Spatial Frequency
- Better Scatter Rejection / Dose Tradeoff?
 - Slot Scan?
 - More Efficient Scatter Grids?

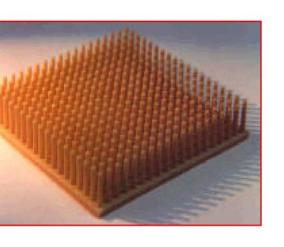
Digital X-Ray Sensors Close to Ideal

Typical Sensor for Ultrasound



Piezoelectric Ceramic

Ultrasound Transducer Needs



Real-Time 3-D Imaging

– 2-D Arrays

Greater Bandwidth

Same Transducer Used for Many Frequencies

Reduce Reflection at Tissue Interface

Match Transducer & Tissue Impedance

Higher Frequency

Higher Resolution ⇒ Small Animal Imaging

Room for Improvement in Many Aspects

Recommendation 1: New Materials

Material Discovery

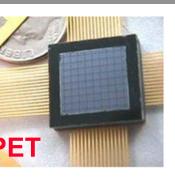
- Scintillators
- Solid State Detectors
- Ultrasound Transducers
- Very Little Current Effort

Material Development

- Difficult & Expensive
 (Minimum 10 years @ \$1M / year for each Material)
- Done by Commercial Sector (if Patent Protected)
- Done by Government (if Not Patent Protected)

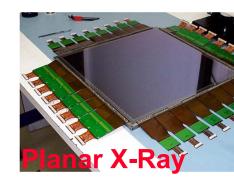
rtually All Modalities Need New Sensor Material

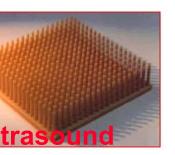
ecommendation 2: Electronics & Packagin



All Modalities Want:

- Larger Area Covered
- Smaller Pixels
- ⇒ Many Pixels (25 million)

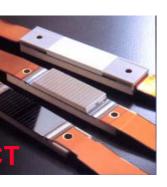




Implications:

- ⇒ High Power Consumption & Density
- ⇒ Large Number & Density of Connections
- ⇒ Modular Design
- ⇒ Dead Area Between Modules
- ⇒ Scintillator Arrays w/ Small Pixels

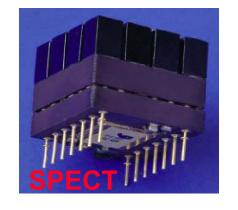




ckaging Improvements Would Help *All* Modalitic



Thanks To:



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